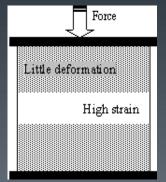


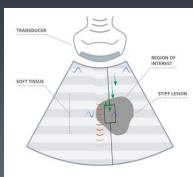
#### EUROSON SCHOOL Eiastography & Interventional US

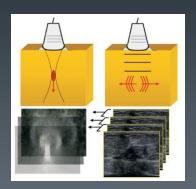


# EFSUMB Guidelines on Elastography: Part I: Basic Principles & Technology

Elena Drakonaki MD, PhD, PostDoc Consultant MSK Radiologist Independent Practice, Heraklion, Greece & Radcliff NHS Trust, Oxford, UK







EUROSON SCHOOL 2014, Athens www.drakonaki.gr

## **US Elastography**

Rapidly evolving in recent years
Growing general interest, a lot of available techniques, level of scientific evidence

#### **EFSUMB**

2011: steering committee selected European experts

Sept 2012: consensus meeting in Bologna

#### Supported by the industry

(BK medical, Echosens, Esaote, GE, Hitachi Aloka, Philips, Siemens, Supersonic, Toshiba)

No influence on the content



Authors

J. Bamber<sup>1</sup>, D. Cosgrove<sup>2</sup>, C. F. Dietrich<sup>3</sup>, J. Fromageau<sup>1</sup>, J. Bojunga<sup>4</sup>, F. Calliada<sup>5</sup>, V. Cantisani<sup>6</sup>, J.-M. Correas<sup>7</sup>, M. D'Onofrio<sup>8</sup>, E. E. Drakonaki<sup>9</sup>, M. Fink<sup>10</sup>, M. Friedrich-Rust<sup>11</sup>, O. H. Gilja<sup>12</sup>, R. F. Havre<sup>13</sup>, C. Jenssen<sup>14</sup>, A. S. Klauser<sup>15</sup>, R. Ohlinger<sup>16</sup>, A. Saftoiu<sup>17</sup>, F. Schaefer<sup>18</sup>, I. Sporea<sup>19</sup>, F. Piscaglia<sup>20</sup>

**Ultraschall Med**. 2013 Apr;34(2):169-84

EFSUMB Guidelines and Recommendations on the Clinical Use of Ultrasound Elastography.
Part 2: Clinical Applications

**Authors** 

D. Cosgrove<sup>1</sup>, F. Piscaglia<sup>2</sup>, J. Bamber<sup>3</sup>, J. Bojunga<sup>4</sup>, J.-M. Correas<sup>5</sup>, O. H. Gilja<sup>6</sup>, A. S. Klauser<sup>7</sup>, I. Sporea<sup>8</sup>, F. Calliada<sup>9</sup>, V. Cantisani<sup>10</sup>, M. D'Onofrio<sup>11</sup>, E. E. Drakonaki<sup>12</sup>, M. Fink<sup>13</sup>, M. Friedrich-Rust<sup>14</sup>, J. Fromageau<sup>3</sup>, R. F. Havre<sup>15</sup>, C. Jenssen<sup>16</sup>, R. Ohlinger<sup>17</sup>, A. Săftoiu<sup>18</sup>, F. Schaefer<sup>19</sup>, C. F. Dietrich<sup>20</sup>

EFSUMB Guidelines and Recommendations on the Clinical Use of Ultrasound Elastography. Part 1: Basic Principles and Technology

**Authors** 

J. Bamber<sup>1</sup>, D. Cosgrove<sup>2</sup>, C. F. Dietrich<sup>3</sup>, J. Fromageau<sup>1</sup>, J. Bojunga<sup>4</sup>, F. Calliada<sup>5</sup>, V. Cantisani<sup>6</sup>, J.-M. Correas<sup>7</sup>, M. D'Onofrio<sup>8</sup>, E. E. Drakonaki<sup>9</sup>, M. Fink<sup>10</sup>, M. Friedrich-Rust<sup>11</sup>, O. H. Gilja<sup>12</sup>, R. F. Havre<sup>13</sup>, C. Jenssen<sup>14</sup>, A. S. Klauser<sup>15</sup>, R. Ohlinger<sup>16</sup>, A. Saftoiu<sup>17</sup>, F. Schaefer<sup>18</sup>, I. Sporea<sup>19</sup>, F. Piscaglia<sup>20</sup>

#### **Outline**

$\overline{}$				
	asic	nrin	OID	
	<b>Jaco</b> lo	$\mathcal{O}$	OID	
			- 1	

- ☐ Quasi-static methods
- □ Dynamic methods
- □ Recommendations
- ☐ Safety issues
- ☐ Appendix-definitions & explanations (online only)

## EFSUMB Guidelines on Elastography: Part I

EUROSON SCHOOL 2014, Athens www.drakonaki.gr

EFSUMB Guidelines and Recommendations on the Clinical Use of Ultrasound Elastography. Part 1: Basic Principles and Technology

**Authors** 

J. Bamber<sup>1</sup>, D. Cosgrove<sup>2</sup>, C. F. Dietrich<sup>3</sup>, J. Fromageau<sup>1</sup>, J. Bojunga<sup>4</sup>, F. Calliada<sup>5</sup>, V. Cantisani<sup>6</sup>, J.-M. Correas<sup>7</sup>, M. D'Onofrio<sup>8</sup>, E. E. Drakonaki<sup>9</sup>, M. Fink<sup>10</sup>, M. Friedrich-Rust<sup>11</sup>, O. H. Gilja<sup>12</sup>, R. F. Havre<sup>13</sup>, C. Jenssen<sup>14</sup>, A. S. Klauser<sup>15</sup>, R. Ohlinger<sup>16</sup>, A. Saftoiu<sup>17</sup>, F. Schaefer<sup>18</sup>, I. Sporea<sup>19</sup>, F. Piscaglia<sup>20</sup>

#### **Outline**

- ☐ Quasi-static methods
- □ Dynamic methods
- □ Recommendations
- ☐ Safety issues
- Appendix-definitions & explanations (online only)

### **Tissue Displacement**

Directly (as distance): ARFI

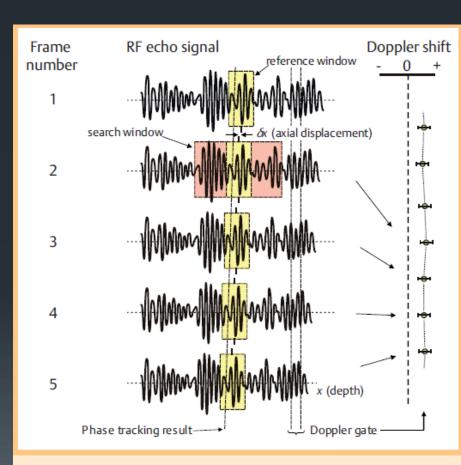
Converted to strain\*: Strain imaging

Calculate the speed of shear waves:

Shear wave

\*Strain: has no units

= the amount of deformation of an
element of the medium compared to
its original size and shape

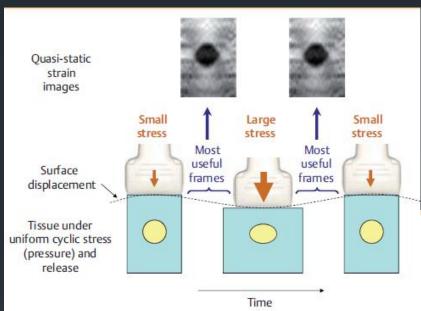


**Fig. 4** The two main methods for estimating displacement used in elastography are RF-echo correlation tracking and Doppler processing. In this

## Strain imaging: Strain Elastography & ARFI (qualitative)

	method	type of force	applied force	property displayed	qualitative/ quantitative	imaging/ measure- ment	commercial implementation	illustration
displacement or strain imaging	strain elasto- graphy (SE) and strain-rate imaging (SRI)	quasi static	mechanically induced – either  active external displacement of tissue surface <sup>1</sup> or  passive internal physiologically induced <sup>2</sup>	strain or strain rate	qualitative, although tools often provided to analyse image characteristics	full area image, refreshed at up to the ultrasound frame rate <sup>3</sup>	Esaote GE Hitachi Aloka Philips Samsung Medison Siemens Toshiba Ultrasonix Zonare	Passive, internal - intrinsic tissue motion
	acoustic radiation force impulse (ARFI) imaging		ultrasound induced – focused radiation force impulse at depth	displace- ment	qualitative	single image within a box	Siemens	Localised displacement at depth from a focused ultrasound radiation force impulse  Dynamic displacement

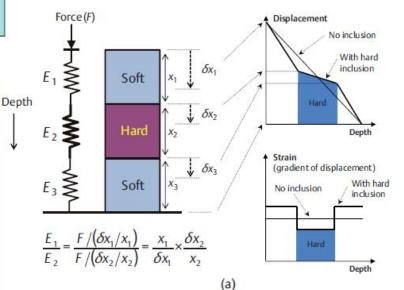
### **Strain Elastography**

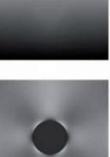


Stress is:

- Transducer induced
- Physiologically induced

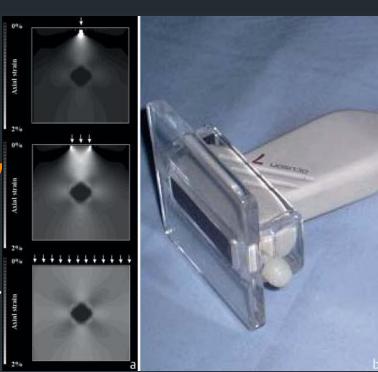
\*Strain: the spatial gradient of displacement, has no units = the amount of deformation of an element of the medium compared to its original size and shape



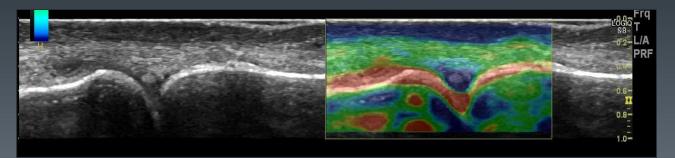


**Small compressor** generates strain of poor penetration and homogeneity

- -footprint extender
- -place a finger on either sides of the transducer and move them with the transducer



Friction between transducer and skin causes less strain (stiff) -more gel needed



## EUROSON SCHOOL 2014, Athens www.drakonaki.gr

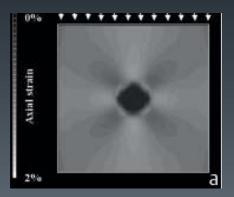
## **Strain Elastography Artefacts**

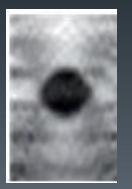
Soft tissue strains more when it is <u>next to hard tissue</u>

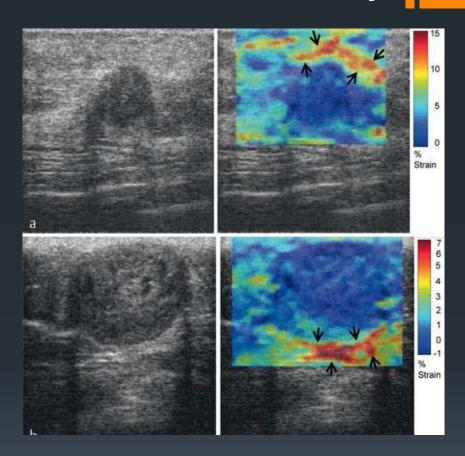
Stress concentration

"Maltese cross" artefacts

(inhomogenous background around a stiff lesion)

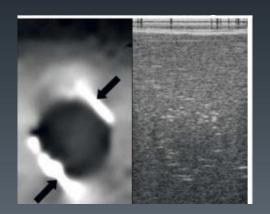


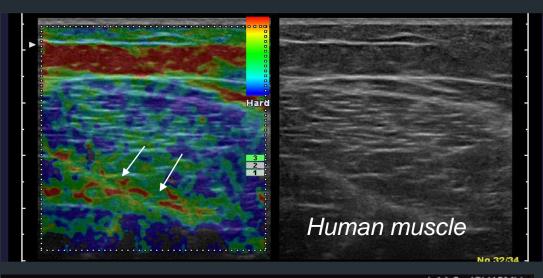


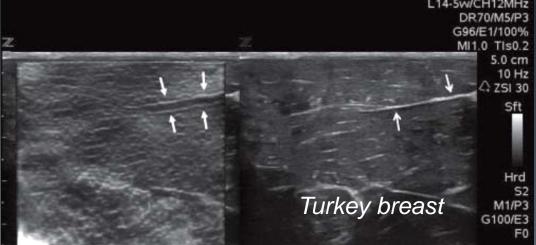


Soft tissue strains more when it is next to a <u>slippery boundary</u>

Edge enhancement artefacts (soft lines around boundaries)







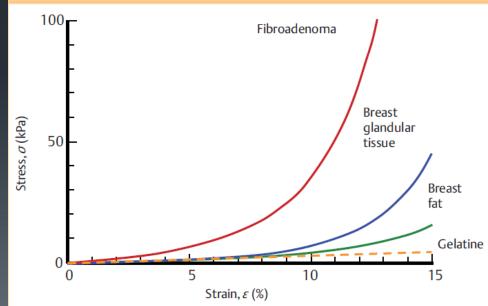
Strain increases with increasing force because tissues are mechanically non linear

Tissue gets harder the more we press and the faster we press

Near constant rate of pressure But not constant pressure

because poroelastic effects will cause the strain image to change with time

Young's modulus=slope of the curve Higher strain – steeper slope

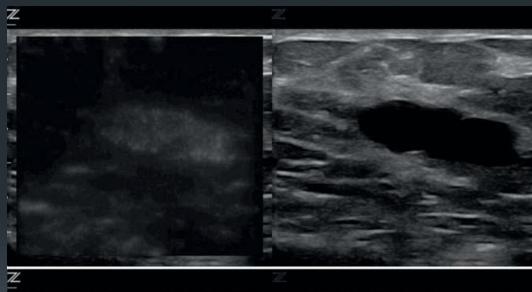


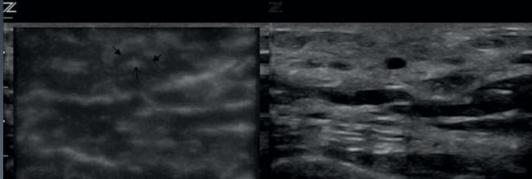
Appearance of cysts varies depending on system settings and the size of the cyst

Small cyst: bulls eye

Big cyst: stop palpating, then switch to high rejection (gain), zero persistence

the cyst filled with strain noise, tissue has zero strain





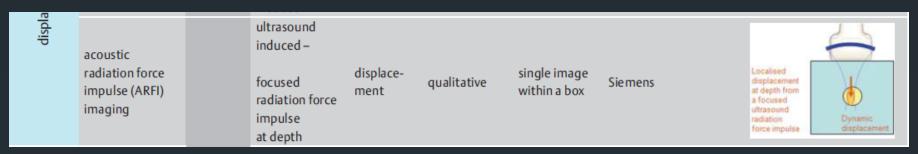
### **Strain Elastography**

#### How to get good quality strain images:

- ► Close proximity to the transducer (< 3 –4cm)
- ▶ Near homogeneous tissue (e. g. liver)
- No anatomical planes that allow slipping
- ► Some distance to tissue boundaries
- ▶ No structures (e. g. large veins) that would damp the shear stress
- ► A broad stress source relative to the width of the imaged region
- ► A limited number of diagnostic targets



### **ARFI** (qualitative image)



Axial displacement caused by a focused US pulse Displacement is displayed directly as a qualitative map

#### Advantages

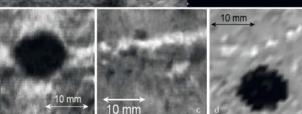
Less operator dependent, Better resolution, Less concentration artefacts, Better SNR at depth, Less influenced by slipping

#### **Drawbacks**

Contrast is easily influenced by the amount of reflection (calcium)

Transducer heating (high power to produce pushing beam)





strain

### **Shear wave speed imaging & measurement**

shear-wave speed MEASUREMENT	transient elasto- graphy (TE) <sup>4</sup>		mechanically induced – impulse ("thump") at tissue surface	shear-wave speed <sup>5</sup>	quantitative	single meas- urement, beam-line average	Echosens	Surface impulse - thumper thumper Shear-wave pulse
shear-wave speed	point shear-wave elastography (pSWE), also known as ARFI quantification <sup>4</sup>	dynamic	ultrasound induced – focused radiation force impulse at depth	shear-wave speed <sup>5</sup>	quantitative	single meas- urement, ROI average	Siemens Philips	Deep shear waves from focused ultrasound radiation force impulse
<u> </u>	shear-wave elas- tography (SWE) <sup>4</sup>		ultrasound induced – radiation force impulses focused at various depths	shear-wave speed <sup>5</sup>	quantitative	single image within a colour box	Siemens	Osep shear waves from focused ultrasound radiation force impulse
		tography (SWE) <sup>4</sup>	ultrasound induced – radiation force focus swept over depth faster than shear-wave speed to create a Mach cone	shear-wave speed <sup>5</sup>	quantitative	image within a colour box, refreshed at up to several per second <sup>3</sup>	SuperSonic Imagine	Deep shear waves from swept-focus ultrasound radiation force Conical shear-wave pulse

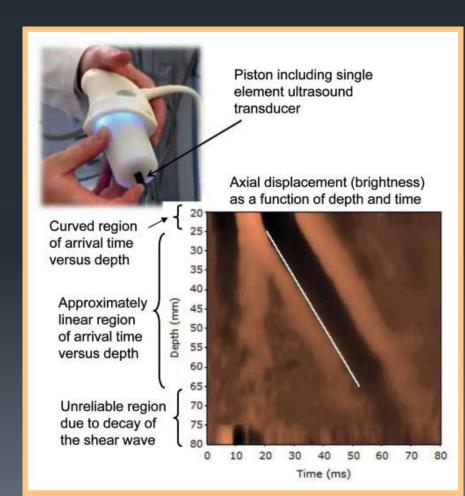
## **Shear wave speed imaging & measurement Transient Elastography**

Short automatic pulse (created by transducer-a piston)

Shear wave speed is measured as the slope and then converted to a Young modulus (kPa)

#### **Echosens system: liver elasticity**

- No conventional US scanner
- Limited by ascites and obesity





## Shear wave speed measurement at a location using ARFI (point SWE)



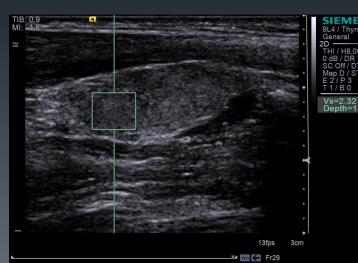
The displacement generated by ARFI creates a transient shear wave

Time of arrival of the shear wave at lateral positions of the ROI

Average SW speed in the ROI is calculated (m/sec) or converted to Young's modulus (kPa)

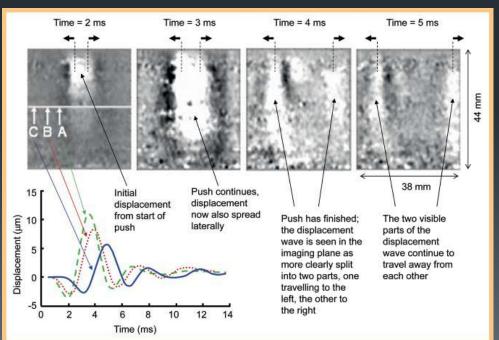
- No elasticity images are produced
- •Depth up to 8 cm
- Possible in ascites, obesity
- Conventional US guidance

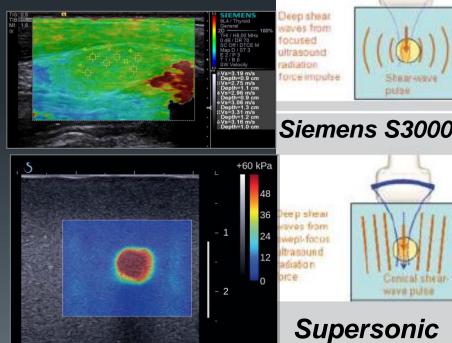
ARFI quantification (Siemens), Philips



### Shear wave speed imaging & measurement Shear wave Elastography

Acoustic radiation force focus is swept down the acoustic axis Generates displacement at all positions along the axis Shear wave in a shape of a cone that travels away





### Shear wave speed imaging & measurement Shear wave Elastography

- Quantitative: speed (m/sec) or Young modulus (kPa)
- No stress concentration artifacts
- •Good penetration (breast 3,5cm, liver 8cm)
- Potentially measure the viscous component

#### limitations

- •Minimize probe pressure (intercostal imaging of liver, no pressure at skin)
- •At interfaces or tissue layers there are other types of waves (Rayleigh, Lamb,

Love waves), artefacts but correction methods are under development

Spatial resolution a little worse than strain and ARFI displacement imaging

#### Elastography types

- Strain imaging (qualitative maps only)
   Strain Elastography, ARFI imaging
- Shear wave speed measurement (measurement only, no image)
   Transient elastography, point ARFI
- Shear wave speed imaging (measurements and image together)
   Siemens S3000 (single image),
   Supersonic Imagine (images refreshed up to several per second)

### Elastography safety issues

#### Strain and shear wave:

identical safety issues as conventional US

#### **ARFI:**

higher TI but within AIUM limits, safety issues similar to Doppler (eye, fetus etc)

#### Conclusion

- Knowledge of physics and technology
- Technology is expected to further develop
- ☐ Improvements are expected in:

image quality
ease of use
quantification methods
tissue characteristics measurable (viscous component)

## EFSUMB Guidelines on Elastography: Part I

## EUROSON SCHOOL 2014, Athens www.drakonaki.gr



Fabio Piscaglia, EFSUMB President, Christoph F Dietrich, EFSUMB President Elect and David Cosgrove First Author of Elastography Guidelines.

J Bamber, Ultrasound and Optics Team, Royal Marsden NHS, UK



Authors and industry at the Elastography meeting in Bologna September 2012.

J. Bamber<sup>1</sup>, D. Cosgrove<sup>2</sup>, C. F. Dietrich<sup>3</sup>, J. Fromageau<sup>1</sup>, J. Bojunga<sup>4</sup>, F. Calliada<sup>5</sup>, V. Cantisani<sup>6</sup>, J.-M. Correas<sup>7</sup>, M. D'Onofrio<sup>8</sup>, E. E. Drakonaki<sup>9</sup>, M. Fink<sup>10</sup>, M. Friedrich-Rust<sup>11</sup>, O. H. Gilja<sup>12</sup>, R. F. Havre<sup>13</sup>, C. Jenssen<sup>14</sup>, A. S. Klauser<sup>15</sup>, R. Ohlinger<sup>16</sup>, A. Saftoiu<sup>17</sup>, F. Schaefer<sup>18</sup>, I. Sporea<sup>19</sup>, F. Piscaglia<sup>20</sup>